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FIG. 1

NULL HYPOTHESIS H	POSSIBILITY OF TRUTH OF NULL HYPOTHESIS H	SIMILARITY OR ABANDONING CRITICAL PROBABILITY $p(x, y)$	WEIGHT $w(p(x, y))$
PIXEL VALUES $v(x) = v(y)$ EXCEPT NOISES OF BOTH PIXELS	LARGE	HIGH	LARGE
	SMALL	LOW	SMALL

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FIG. 2

RADIOGRAPHIC MEANS		SUBJECT FOR AND PURPOSE OF RADIOGRAPHING	PURPOSE OF COHERENT FILTER	METHOD OF CONSTRUCTING $v(x)$
EQUIPMENT	RADIOGRAPHIC METHOD			
X-RAY CT	DYNAMIC CT	TO OBSERVE DYNAMIC CHANGE	TO REDUCE NOISES WITHOUT SPOILING SPATIAL AND TEMPORAL RESOLUTIONS	PIXEL VALUES $v_k(x)$ ARE CALCULATED FROM PLURALITY OF (k) IMAGES OF IDENTICAL PART
MRI	DYNAMIC MRI	DITTO		
SPECT	DYNAMIC SPECT	DITTO		
PET	DYNAMIC PET	DITTO		
RADIOGRAPHY	FLUOROSCOPY	DITTO		
X-RAY CT	PLURALITY OF TIMES OF RADIOGRAPHING	TO OBTAIN IMAGE OF HIGH S/N RATIO	DITTO	DITTO
MRI	DITTO	DITTO		
SPECT	DITTO	DITTO		
PET	DITTO	DITTO		
GAMMA CAMERA RADIOGRAPHY	DITTO	DITTO		
X-RAY CT	MULTICHANNEL RADIOGRAPHING	TO OBTAIN MANY SORTS OF IMAGES OF HIGH S/N RATIO	DITTO	PIXEL VALUES ARE CALCULATED FROM PLURALITY OF SORTS OF IMAGES. AS TO SORTS $k$ ( $k = 1, \dots, K$ ), $v(x) = (v_1(x), v_2(x), \dots, v_k(x))$ IS CALCULATED FROM SCALAR VALUES $v_k(x)$ AT SAME PARTS OF IMAGES $k$ .
MRI	RADIOGRAPHING BASED ON MANY SORTS OF PULSE SEQUENCES	DITTO		
SPECT	MULTIWINDOW RADIOGRAPHING	DITTO		
PET	DITTO	DITTO		
COLOR CAMERA	COLOR RADIOGRAPHING	TO OBTAIN COLOR IMAGE OF HIGH S/N RATIO		

(CONT.)

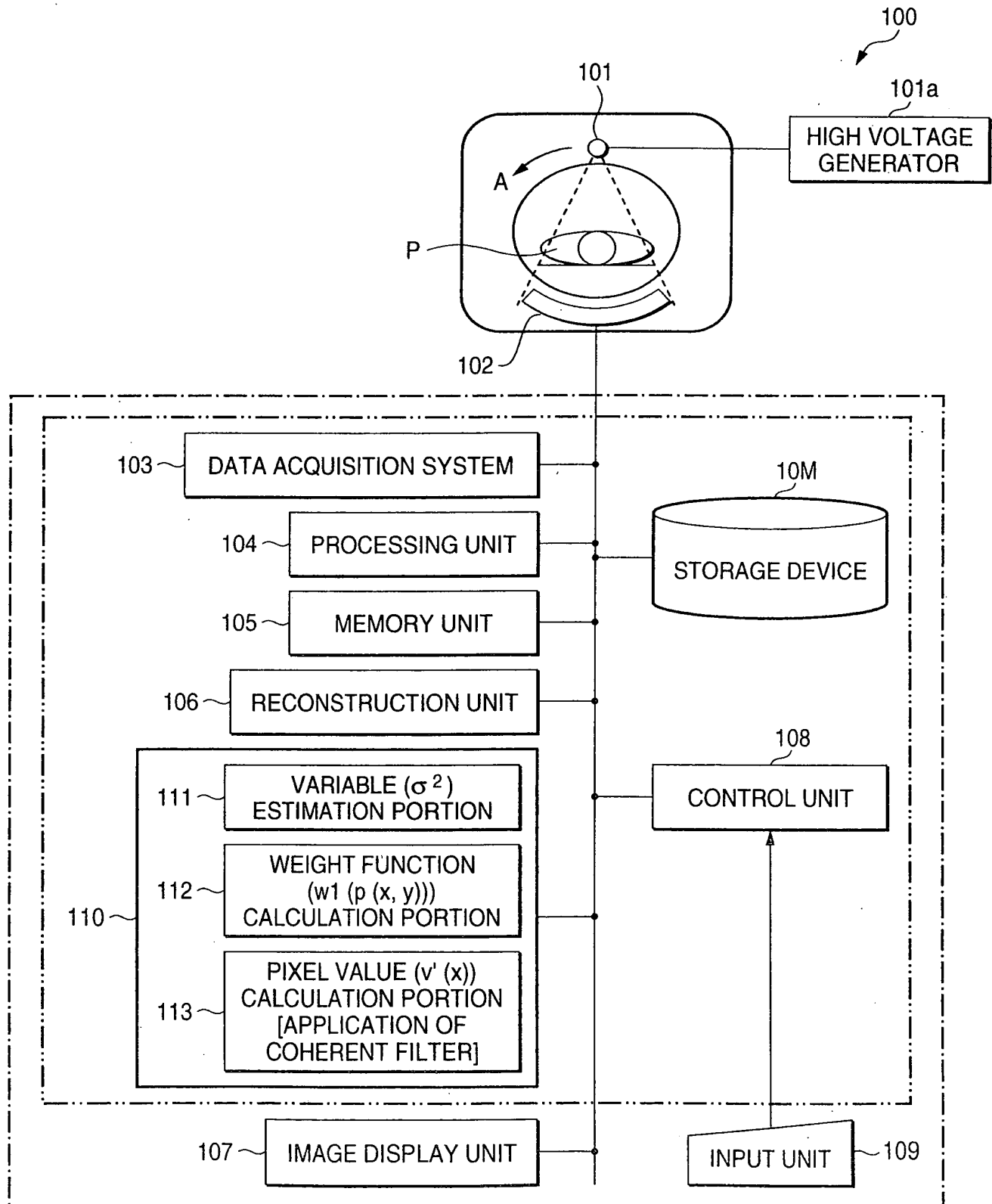
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(FIG. 2 CONTINUED)

ALL RADIO- GRAPHING EQUIPMENT	ALL RADIOGRAPHING METHODS	TO OBTAIN IMAGE OF HIGH S/N RATIO	DITTO	VECTOR VALUES $v(x)$ OF PIXEL $x$ IS CALCULATED AS $v(x)$ $= (v(y_1), v(y_2), \dots, v(y_k) \cdot v(x))$ BY USING SCALAR VALUES OF PIXEL $Z(x) = \{y_1, y_2, \dots, y_k \cdot x\}$ CONTAINED IN VICINITY $Z(x)$ OF $x$
SPECT, PET, X-RAY CT, MRI	3D VOLUME RADIOGRAPHING	TO OBTAIN IMAGE OF HIGH S/N RATIO	DITTO	VECTOR VALUES $v(x)$ OF PIXEL $x$ IS CALCULATED AS $v(x) =$ $(v(y_1), v(y_2), \dots, v(y_k) \cdot v(x))$ BY USING SCALAR VALUES OF PIXEL $Z(x) = \{y_1, y_2, \dots, y_k \cdot x\}$ CONTAINED IN VICINITY $Z(x)$ OF $x$ . IN CASE OF 3D RADIOGRAPHING, $z$ IS IN THREE-DIMENSIONAL VICINITY

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FIG. 3



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FIG. 4 (a)

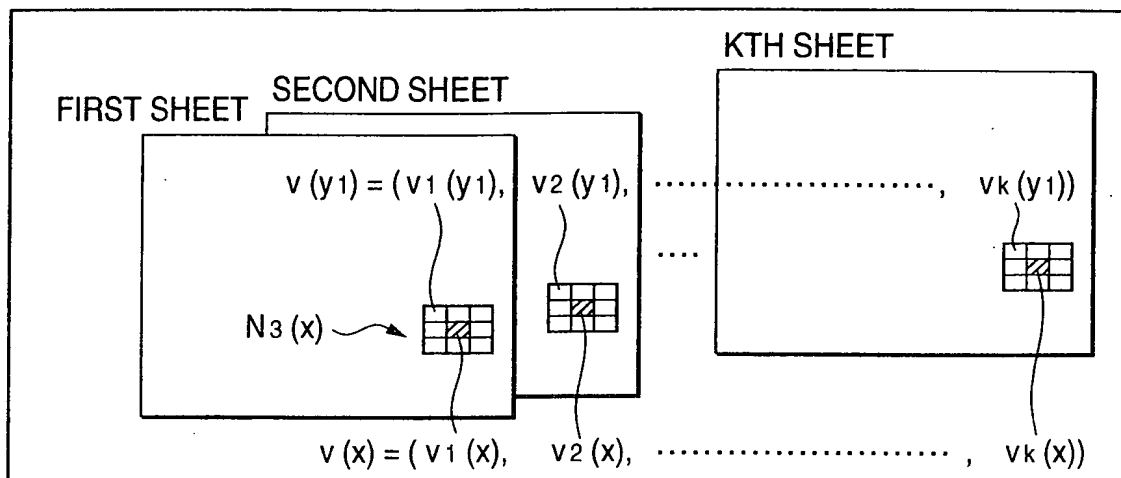


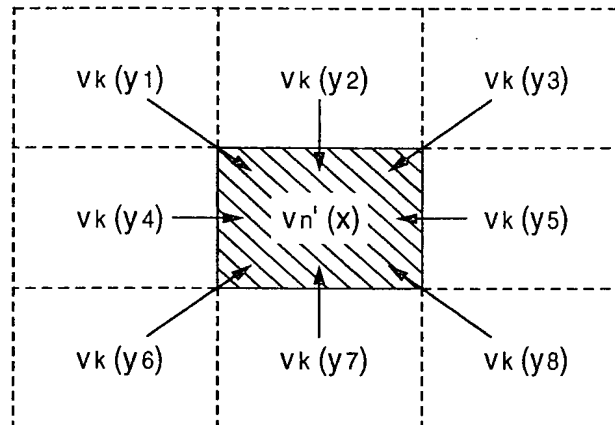
FIG. 4 (b)

WEIGHTS CONCERNING PIXELS  $y_1$ - $y_8$   
AND  $x$  AS CALCULATED FOR SET  $N^{3 \times 3}(x)$

$w1(p(x, y1))$	$w1(p(x, y2))$	$w1(p(x, y3))$
$w1(p(x, y4))$	$w1(p(x, y))$	$w1(p(x, y5))$
$w1(p(x, y6))$	$w1(p(x, y7))$	$w1(p(x, y8))$

FIG. 4 (c)

$v'_k(x)$  CALCULATED FROM  
 $v_k(y1) - v_k(y8)$  AND  $v_k(x)$  IN KTH IMAGE



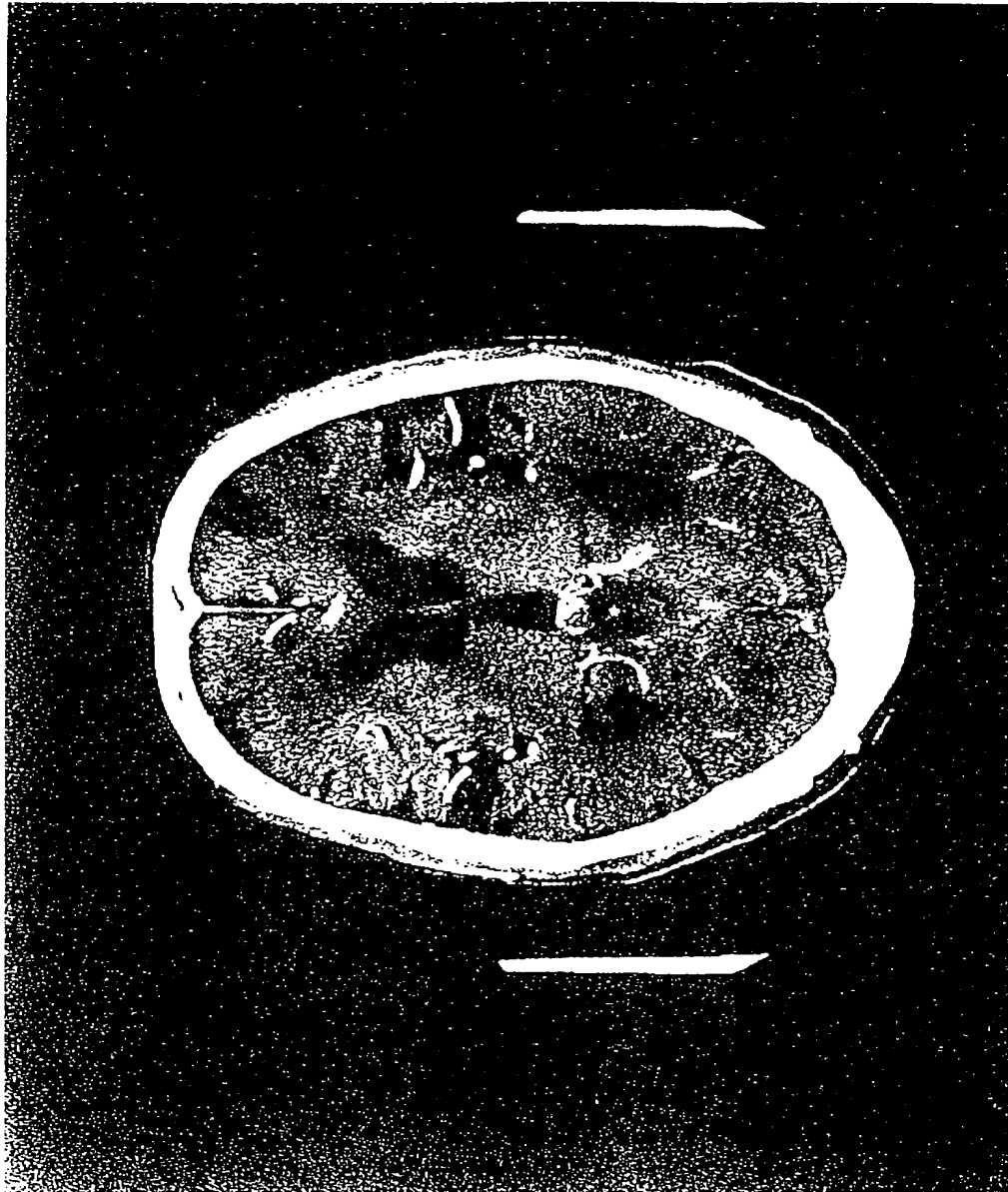
FOR K STATIC IMAGES IN FIGURE

$$w1(p(x, y)) = \exp \left[ - \left\{ \frac{\sqrt{\sum_{k=1}^K \frac{\{v_k(x) - v_k(y)\}^2}{K}}}{2\sigma} \right\}^c \right]$$

$$v'_k(x) = \frac{\sum_{y \in (y1, \dots, y8, x)} v_k(y) \cdot w1(p(x, y))}{\sum_{y \in (y1, \dots, y8, x)} w1(p(x, y))}$$

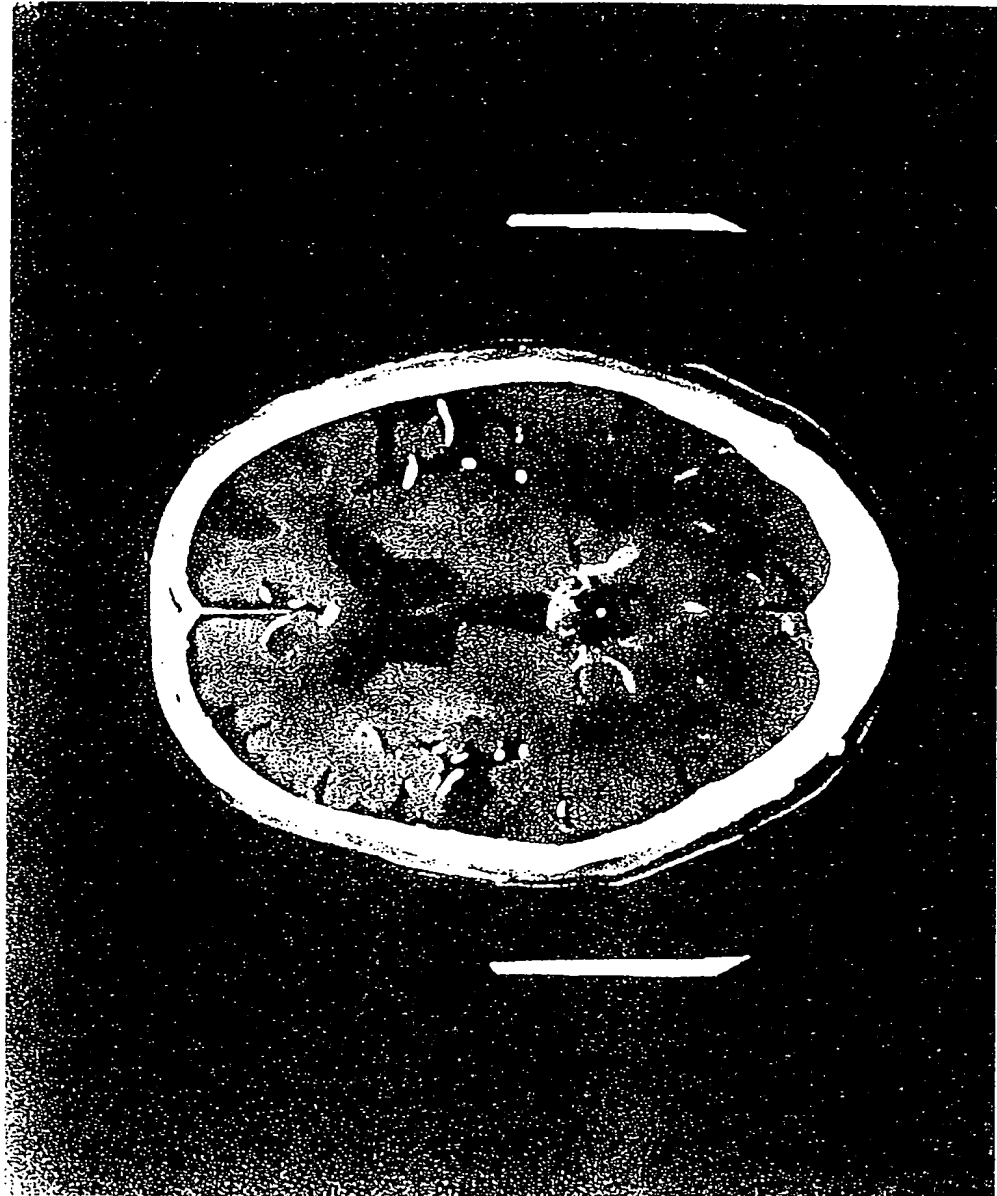
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FIG. 5 (a)



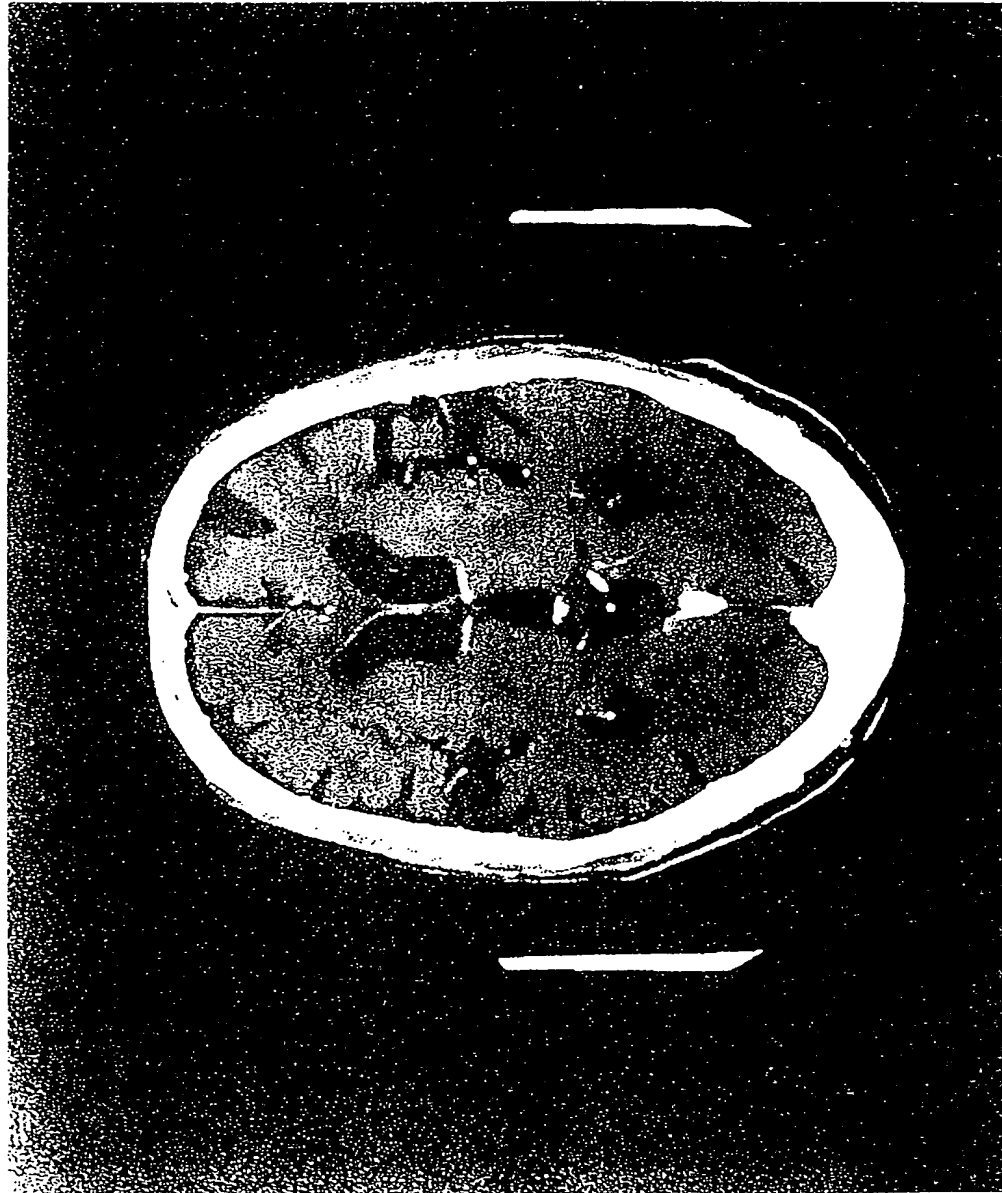
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FIG. 5 (b)



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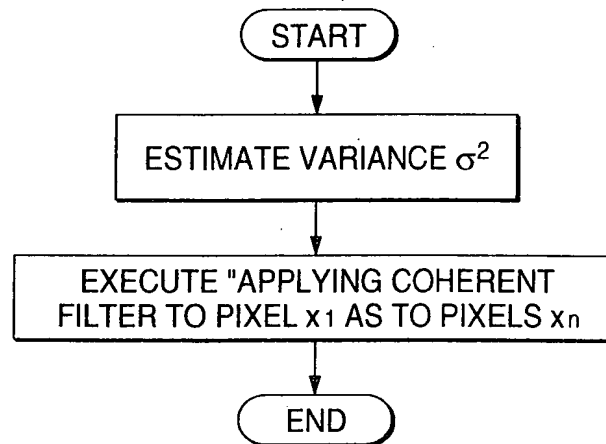
FIG. 5 (c)



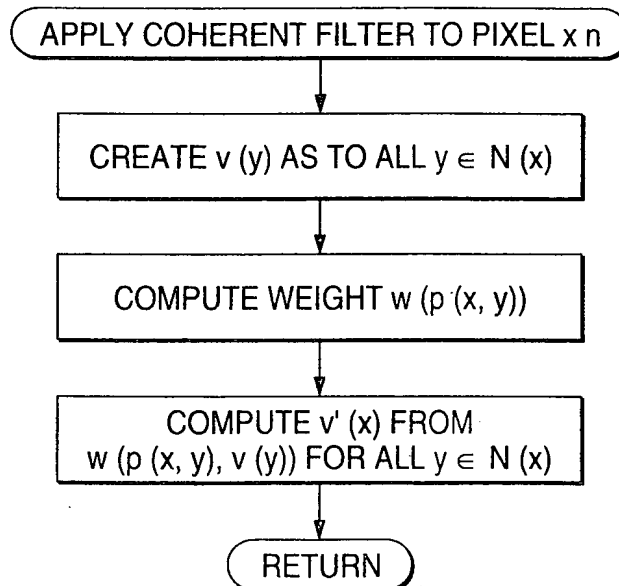


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*FIG. 6 (a)*

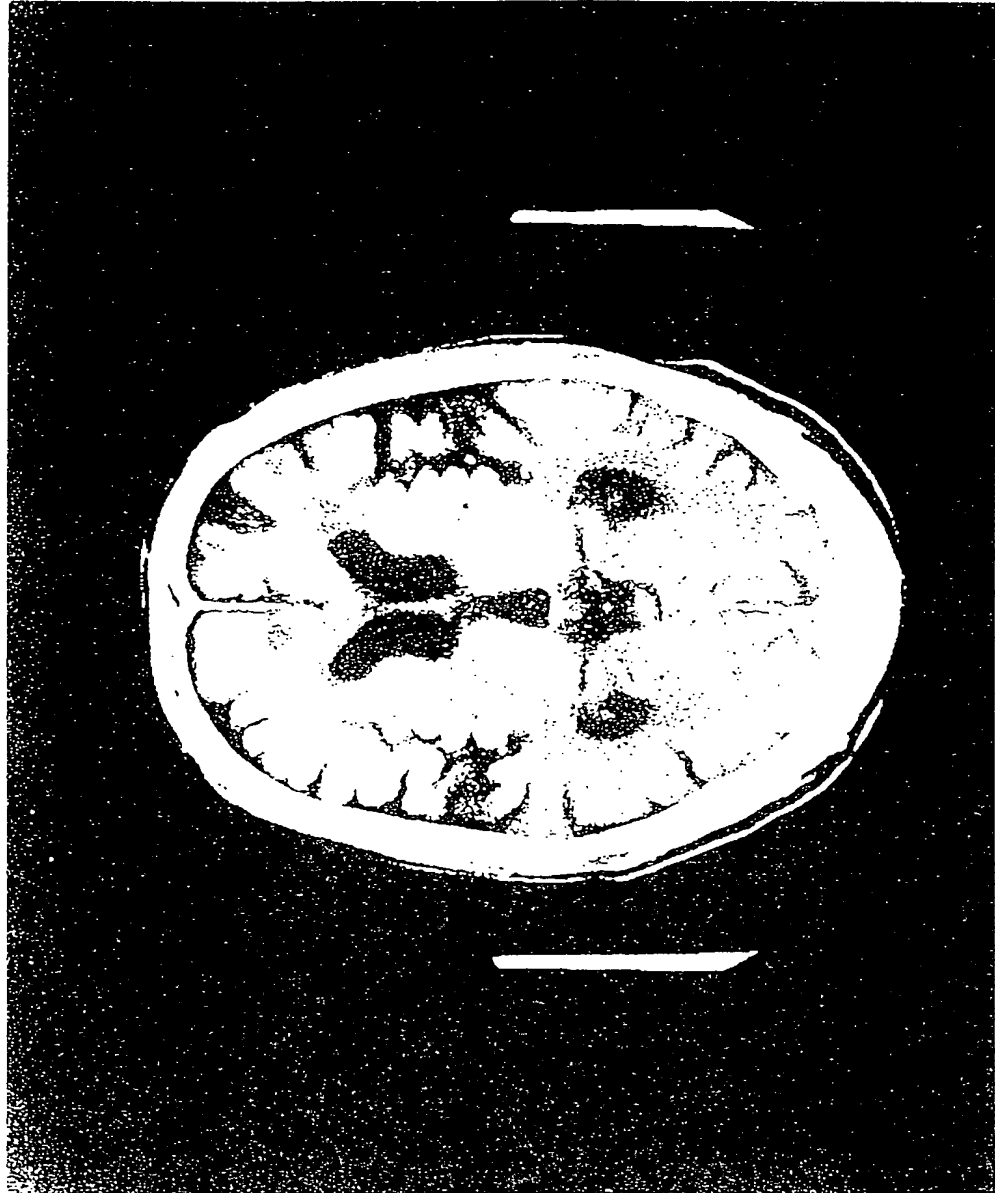


*FIG. 6 (b)*



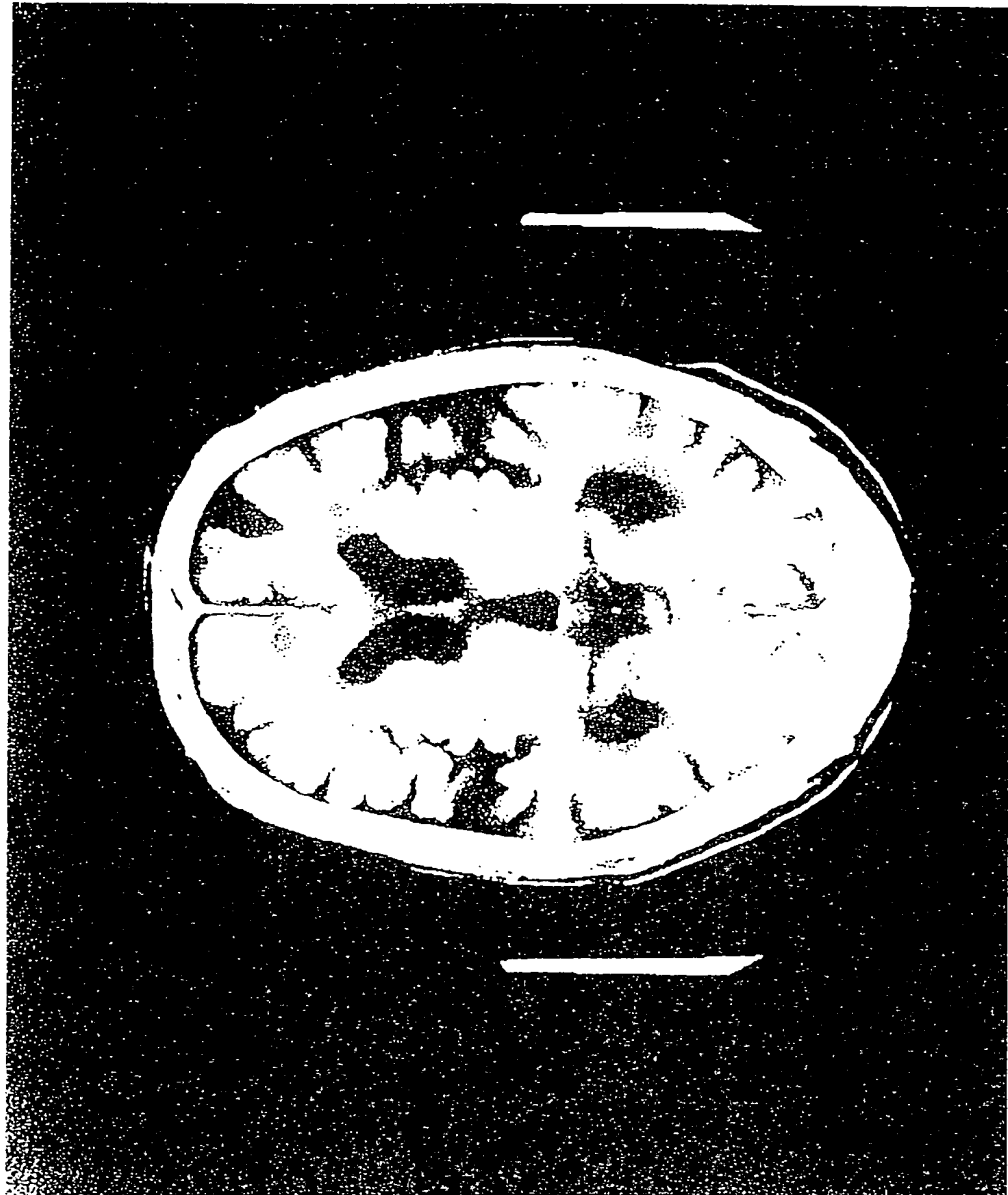
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FIG. 7 (a)



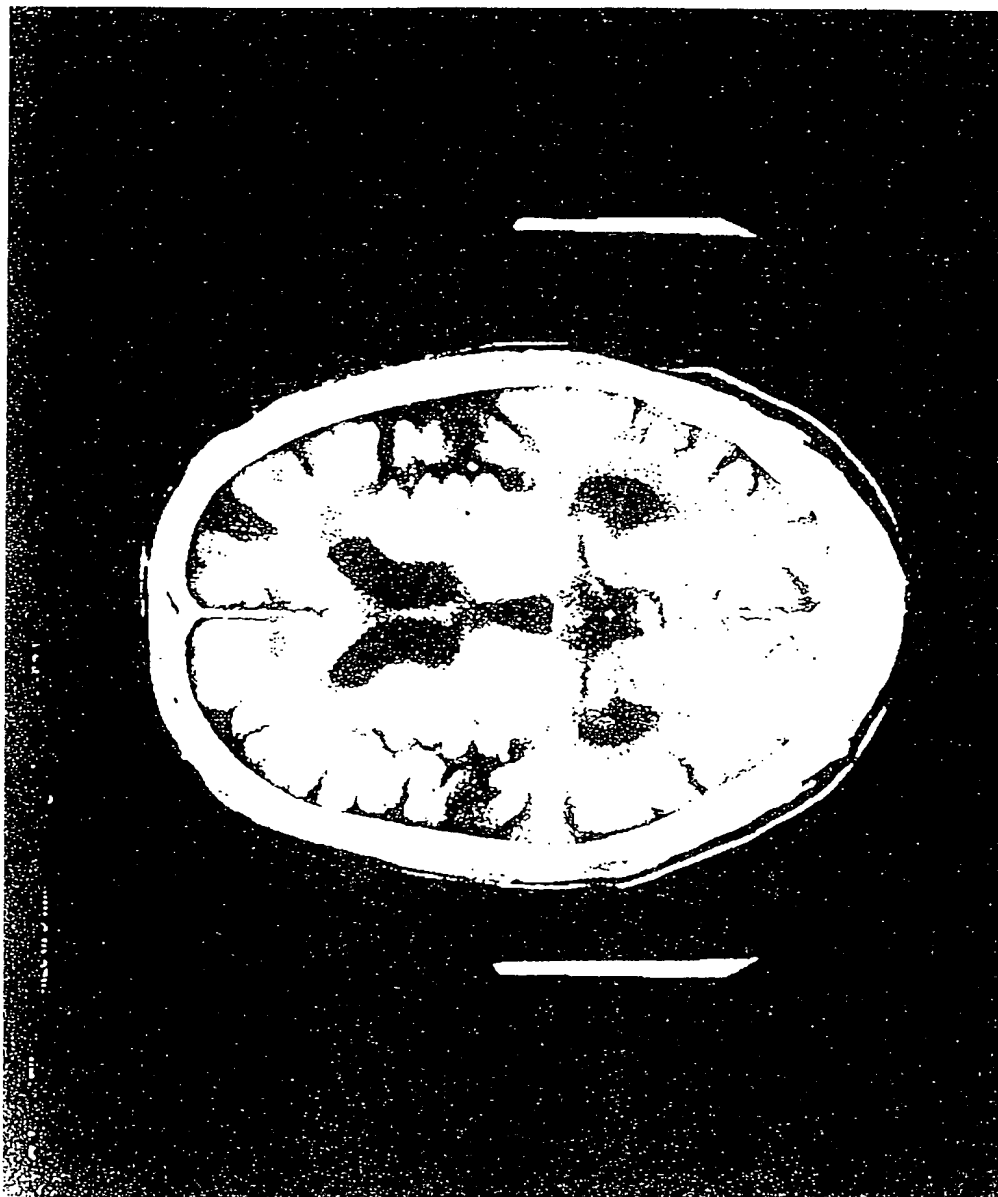
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FIG. 7 (b)



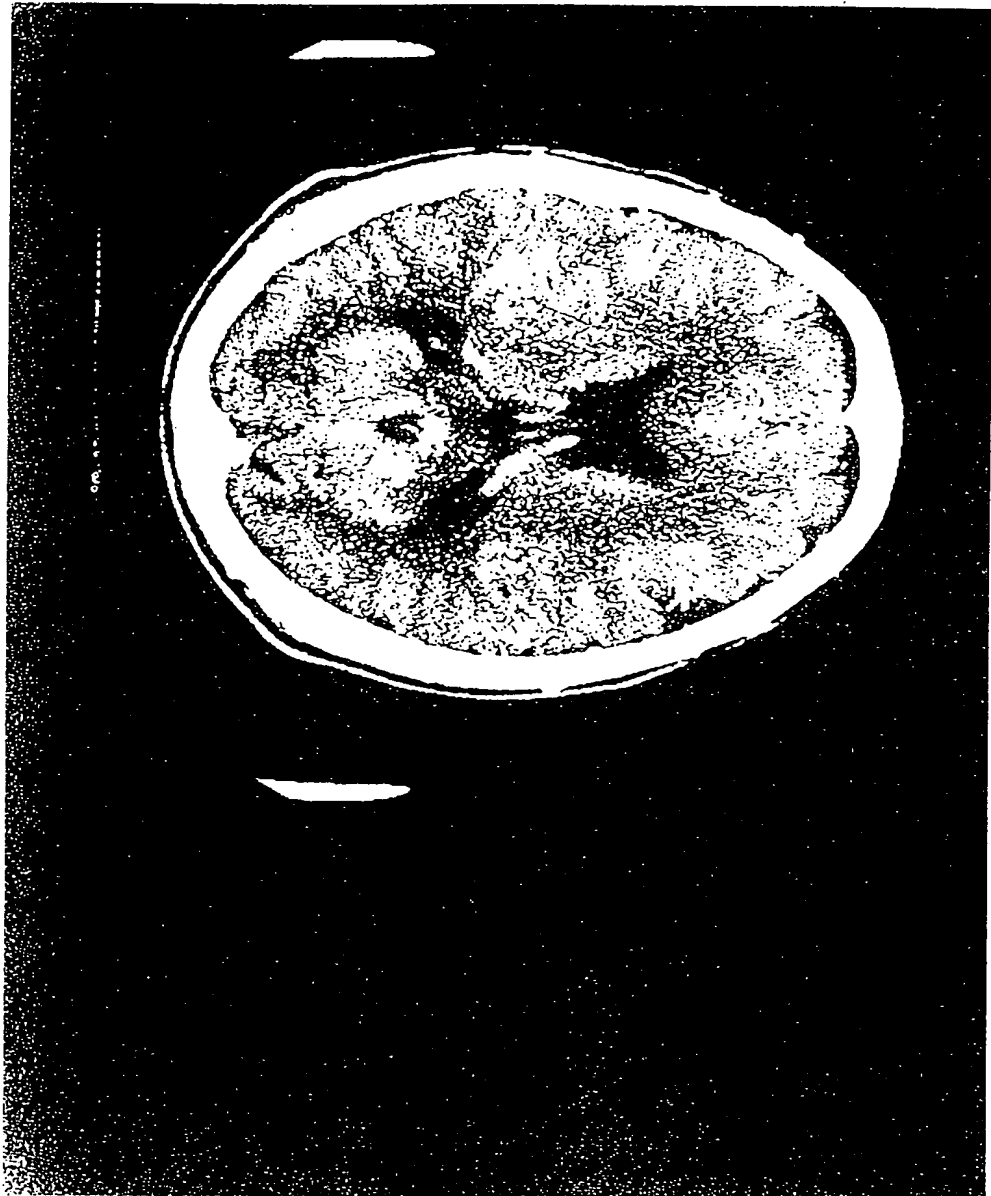
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FIG. 7 (c)



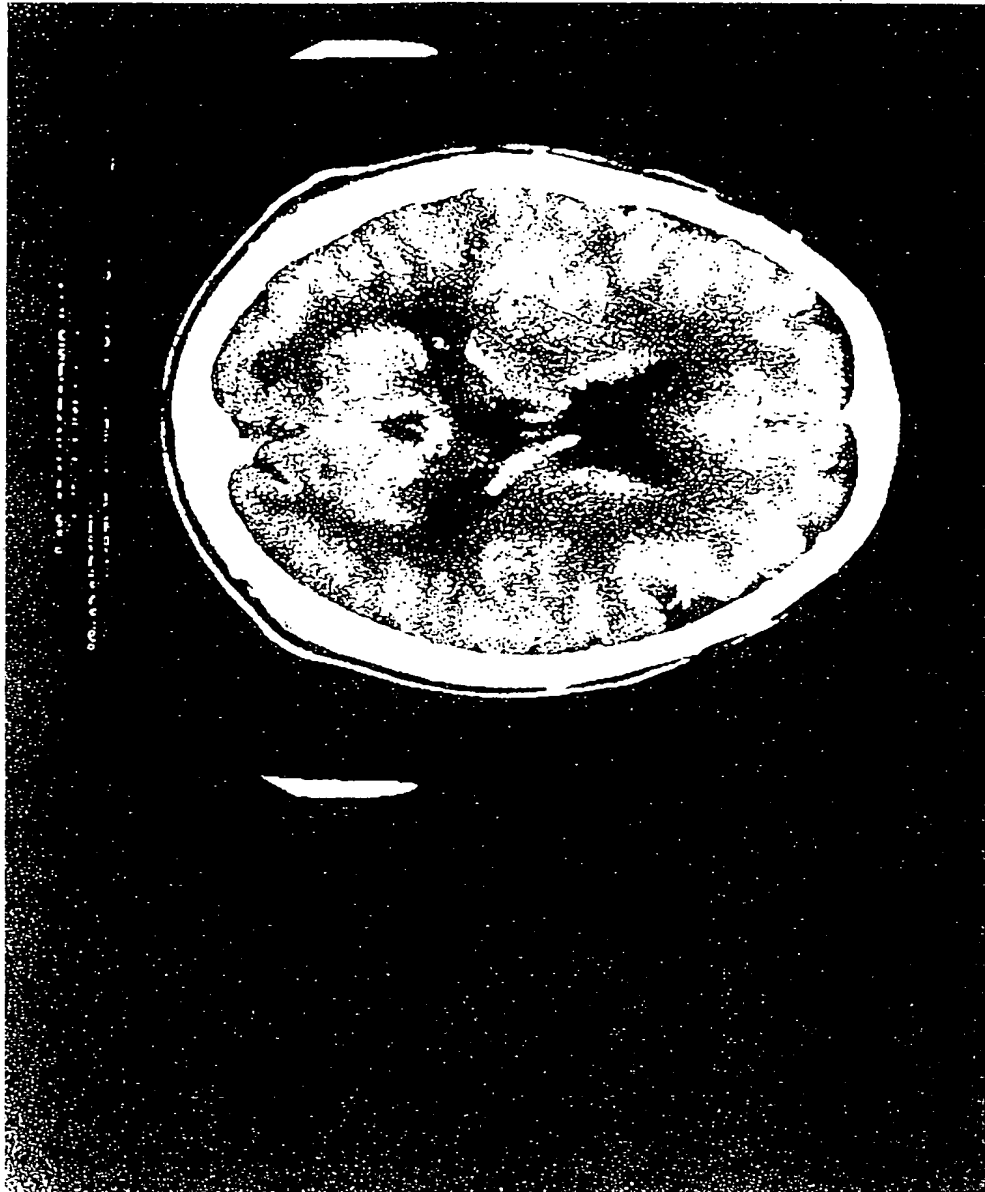
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FIG. 8 (a)



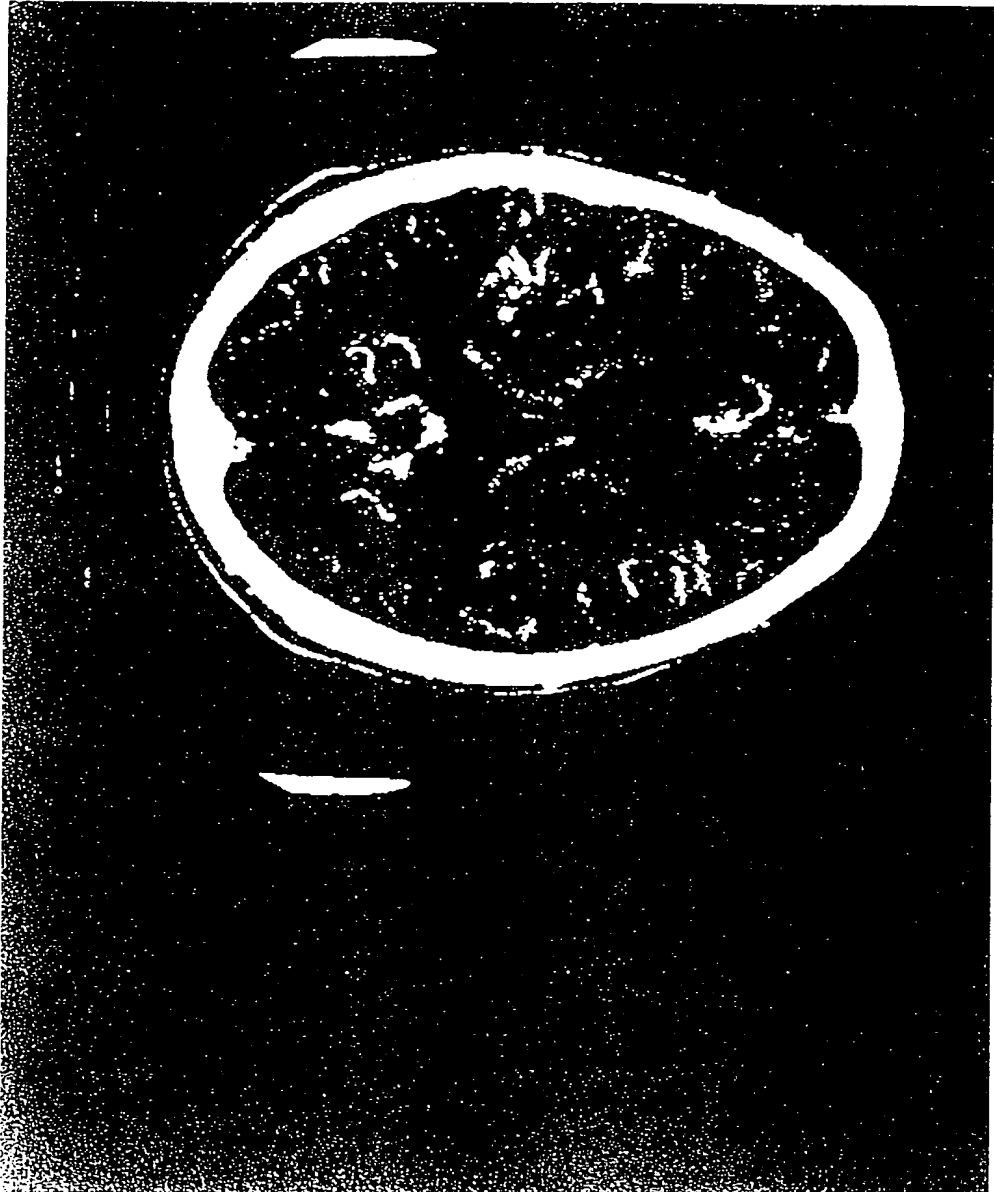
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FIG. 8 (b)



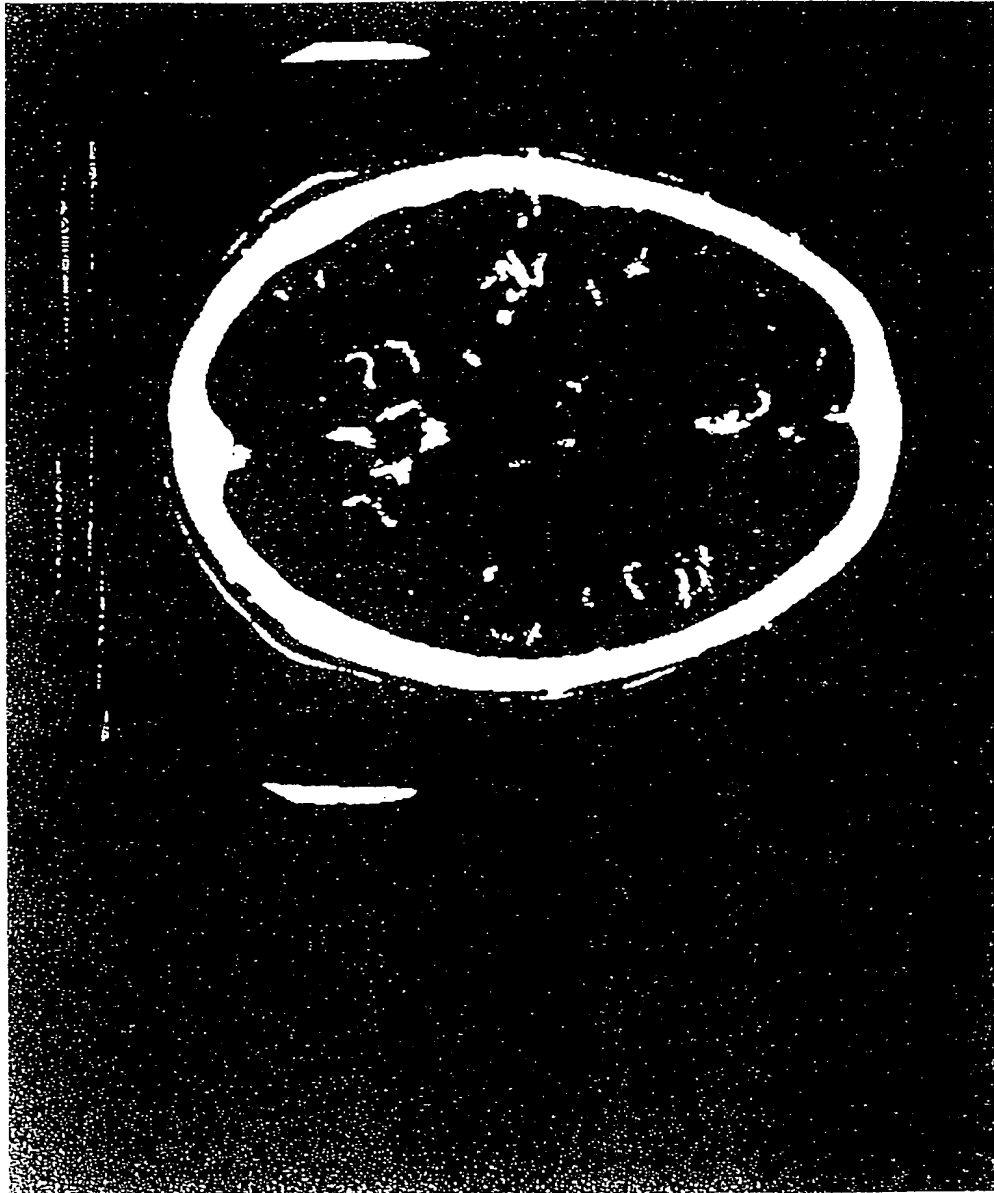
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FIG. 8 (c)



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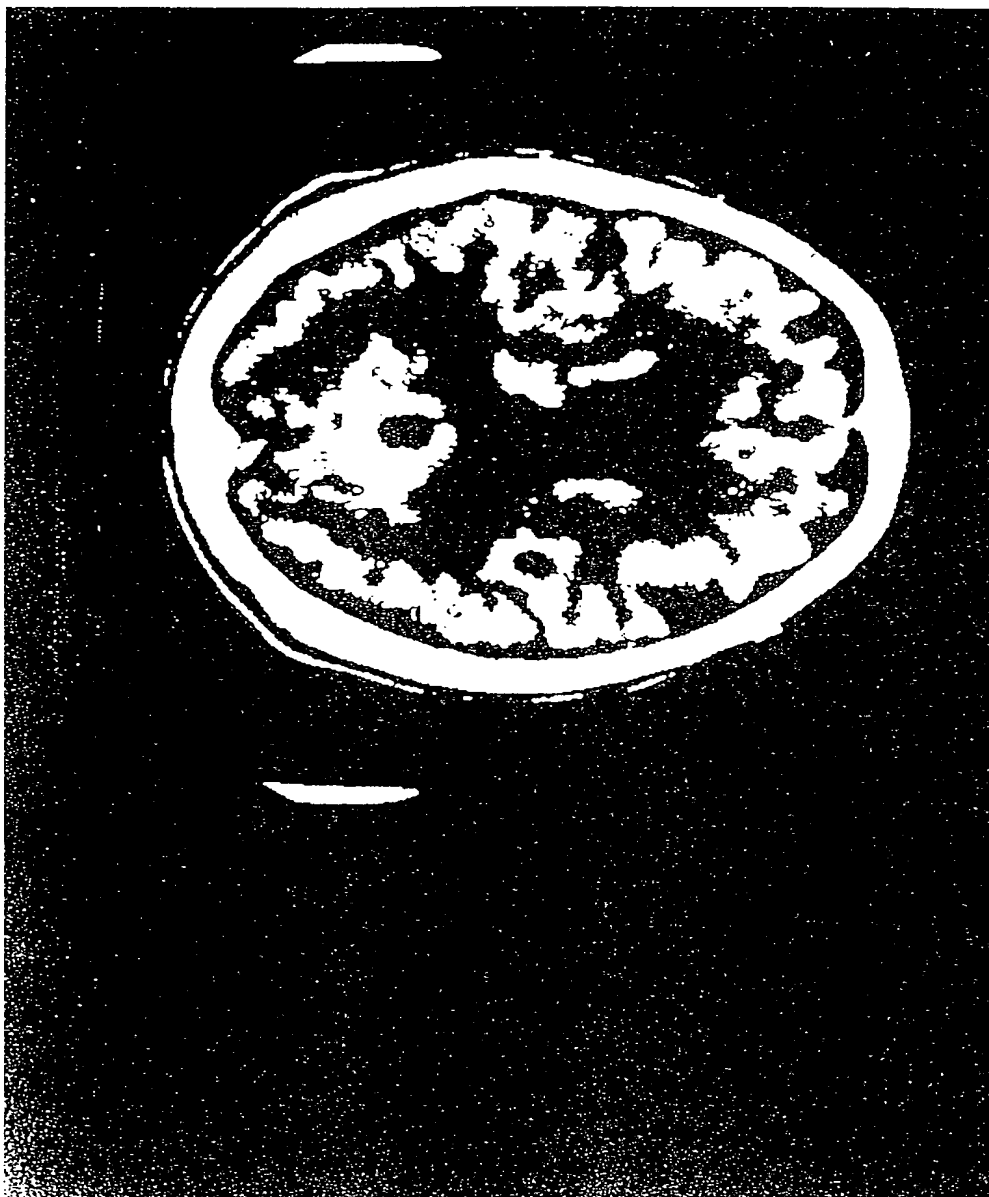
FIG. 8 (d)





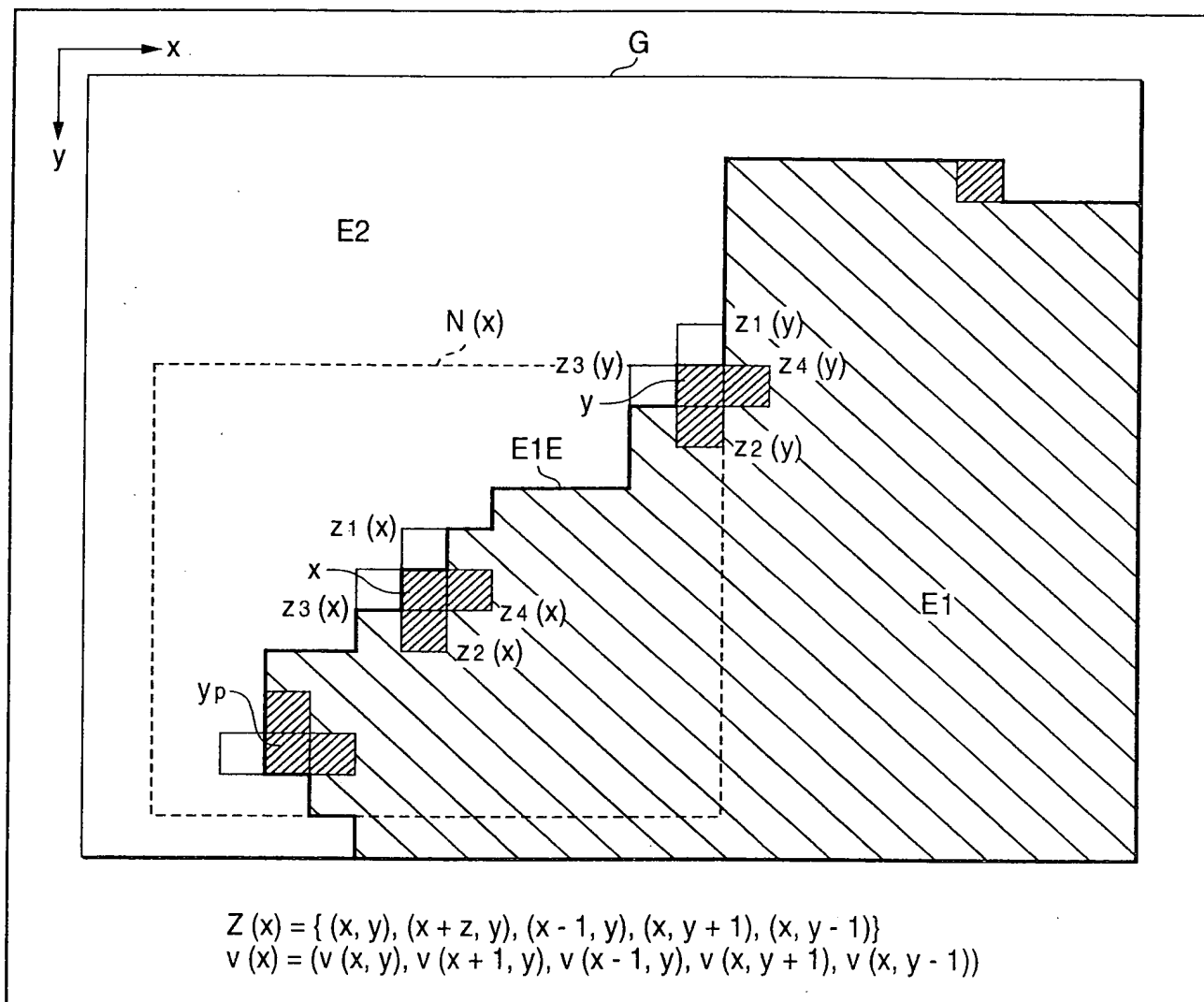
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FIG. 8 (e)



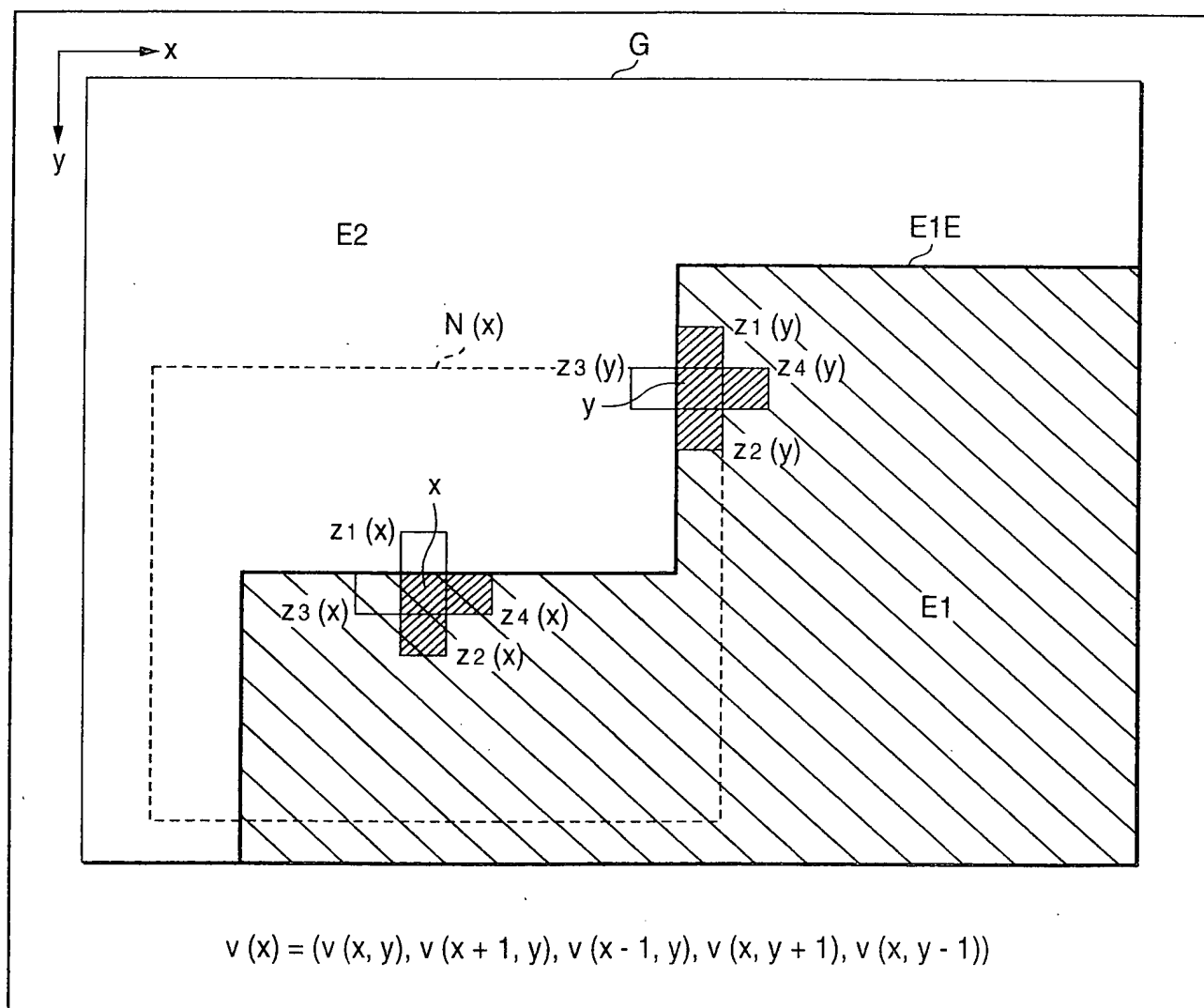
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FIG. 9



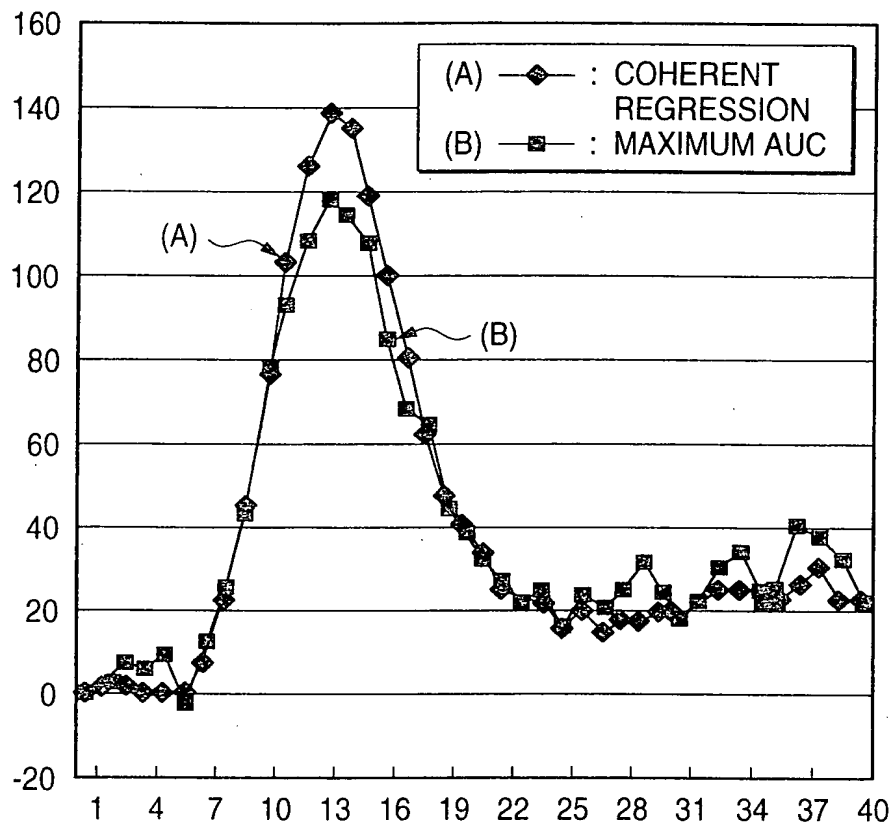
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FIG. 10



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FIG. 11



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FIG. 12 (a)

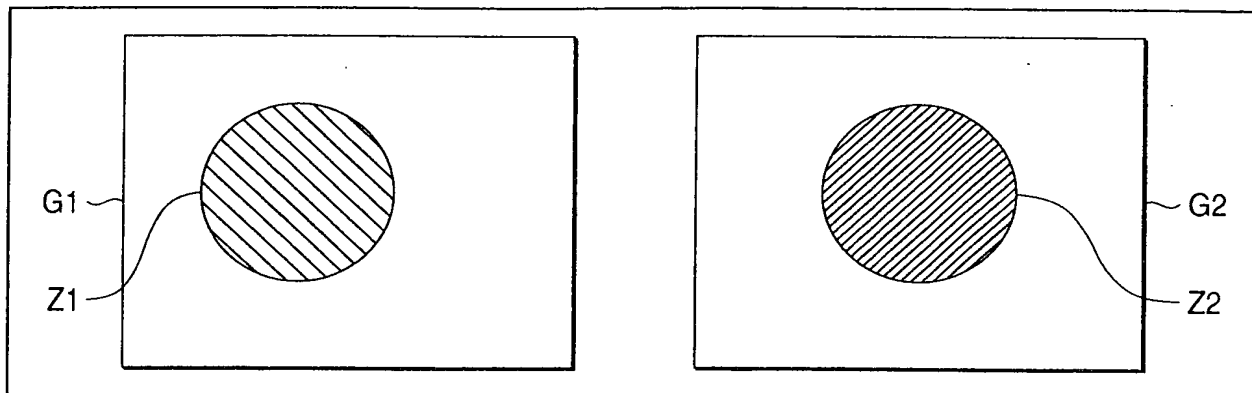


FIG. 12 (b)

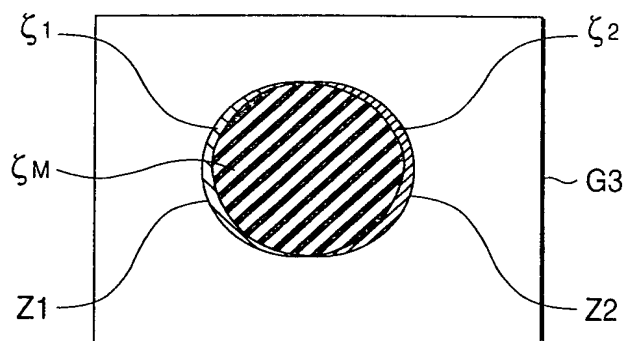
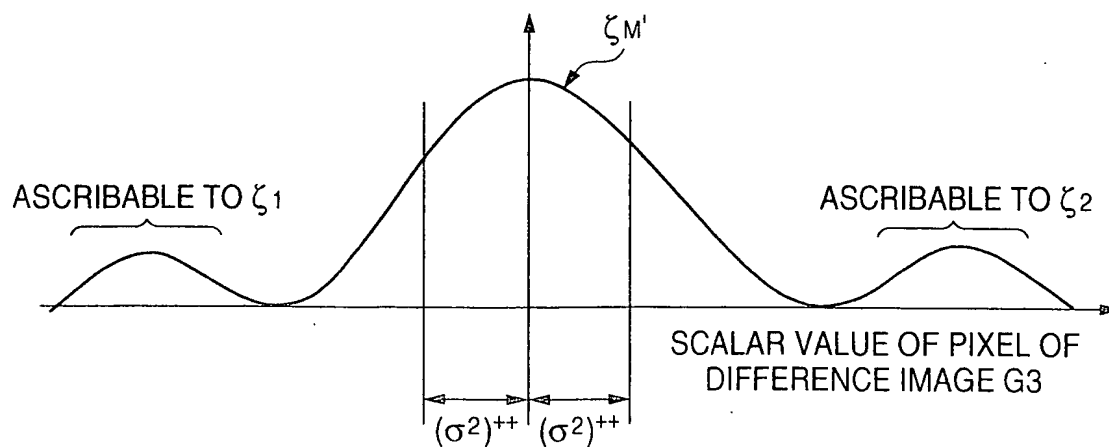


FIG. 12 (c)



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FIG. 13

